

# Anisotropic Elastomers for Polymer Heart Valves

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# POLYMER HEART VALVE TEAM



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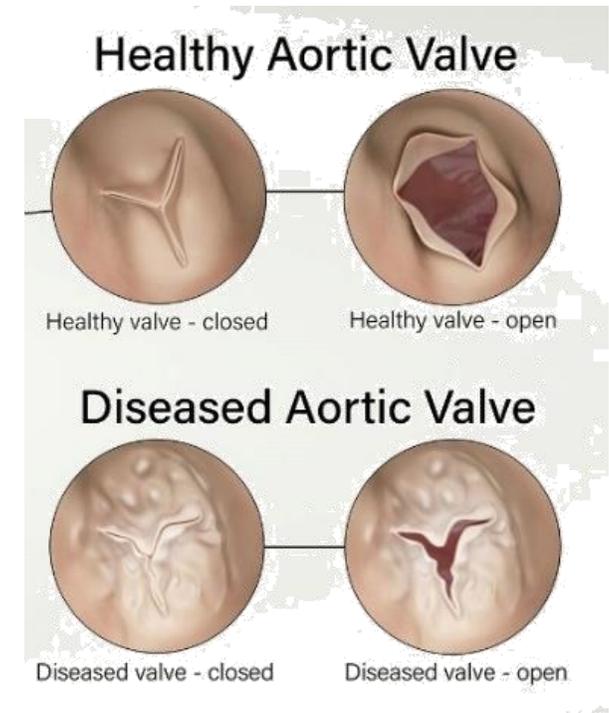
Eugenia Biral



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# HEART VALVE DISEASE

- Valvular heart disease (VHD) affects over 100 million people globally
- Aortic valve disease is the most prevalent VHD
- Types:
  - Stenosis: heart valve does not open fully
  - Regurgitation: heart valve does not close fully
- Causes:
  - Congenital conditions
  - Degenerative conditions



Source: <https://patientdecisionaid.org/aortic-stenosis/>

**Clinical treatment:** Heart valve replacement surgery → 500,000 a year, a figure expected to double in the next 50 years

# CURRENT HEART VALVE PROSTHESIS

## Mechanical replacements

- Hard, man-made materials
- ✓ Long-term durability (~20 years)
- ✗ Requires patient to take life-long anticoagulants



## Biological replacements

- Porcine or bovine tissue leaflets
- ✓ Biocompatibility
- ✗ Lower durability (10-15 years), leading to repeat operation

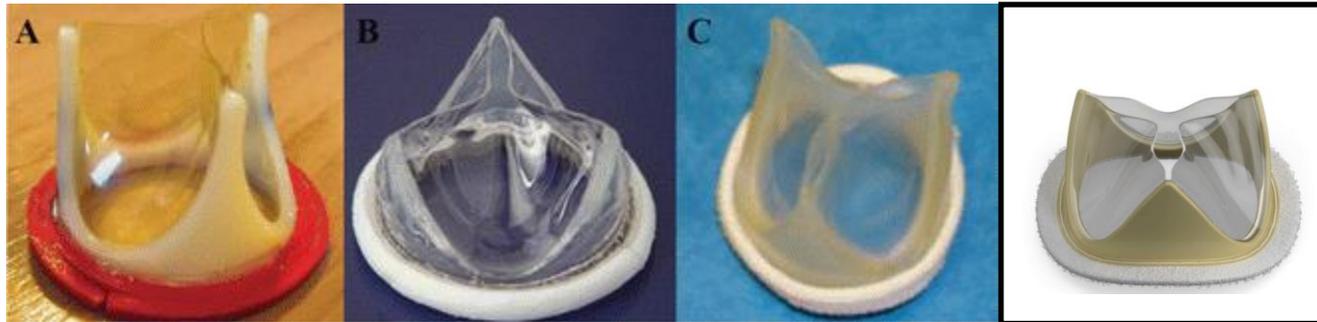


**Research aim:** To meet the need for a prosthesis that is suitable for all patients

# POLYMER HEART VALVES

**A potential solution:** A flexible leaflet polymer heart valve (PHV) that mimics the hemodynamic performance of the native heart valve

Materials used in different attempts to design a PHV:



- MM Rozeik et al. *The aortic valve: structure, complications and implications for- Foldax, Tria heart valve, transcatheter aortic valve replacement*, 2014. Source: <https://foldax.com>

**Silicone**

**Polyurethanes**

**Polytetrafluoroethylene  
(PTFE)**

**Polyesters (e.g. PET)**

**Styrenic thermoplastic  
elastomers**

# POLYMER HEART VALVES

## Opportunities:

- Cheaper and easier to manufacture
- Potential for no anticoagulation therapy

## Limitations so far:

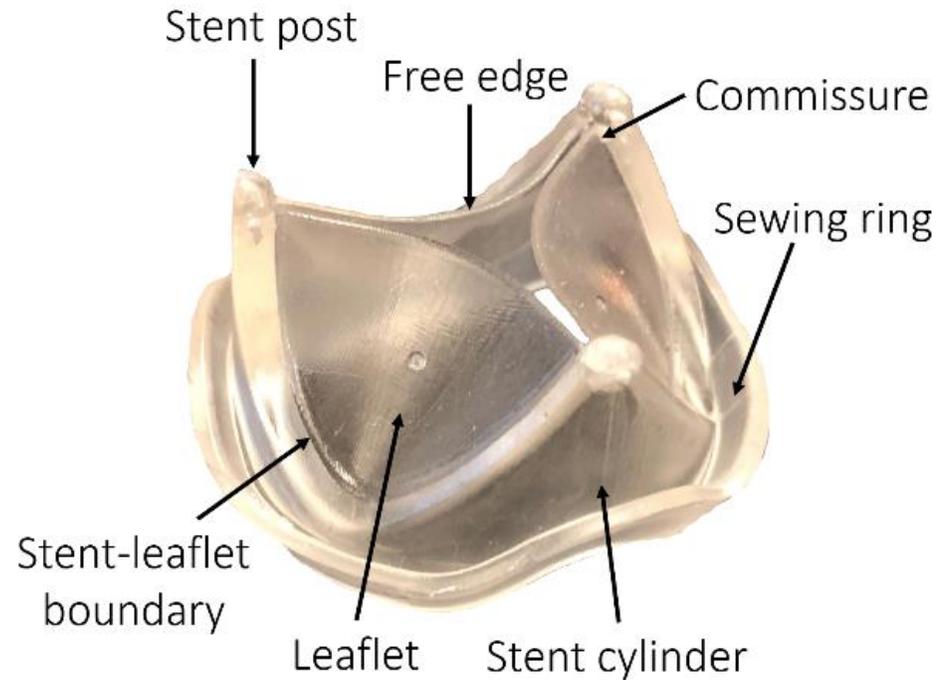
- Mechanical failure (tearing of leaflets)
- Calcification



**How can durability be improved?**

# POLIVALVE

**Surgical PoliValve** – An entirely **injection moulded** polymer heart valve made from styrenic thermoplastic elastomers, designed and developed by the Structured Materials group

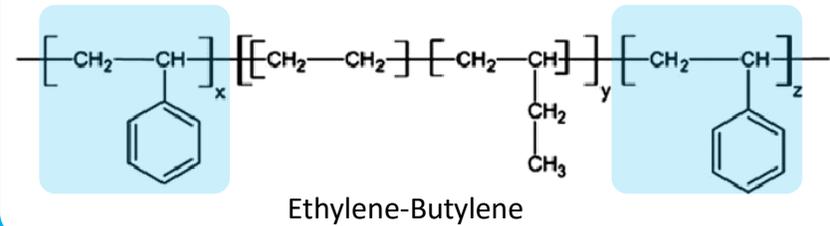


# STYRENIC THERMOPLASTIC ELASTOMERS

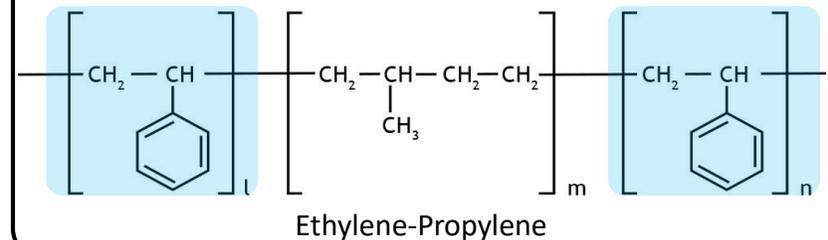
- PoliValve is made of thermoplastic elastomers (SEBS grades)
- These are block copolymers which phase separate
- Styrene blocks forms hard, crystalline phases
- Central blocks form soft, rubbery phases

**Varying functional group, styrene content and molecular weight strongly affects material performance**

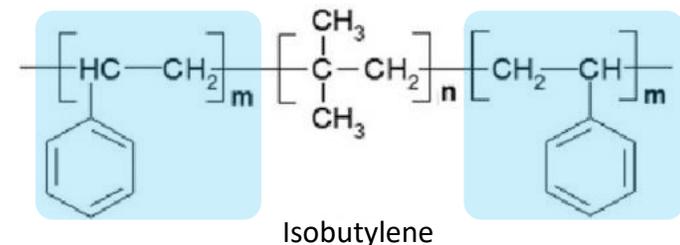
## SEBS



## SEPS



## SIBS



# STYRENIC THERMOPLASTIC ELASTOMERS

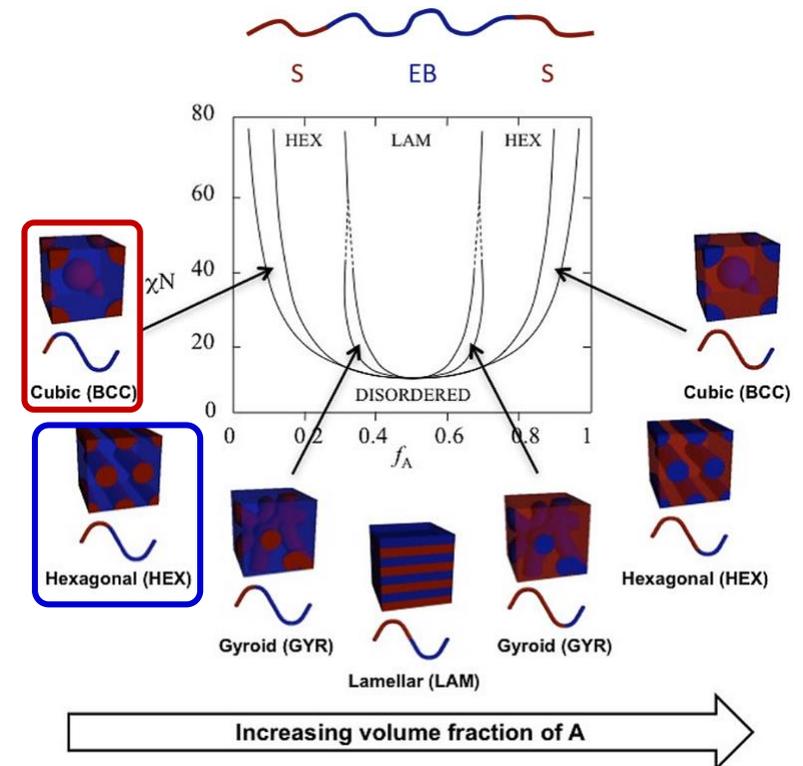
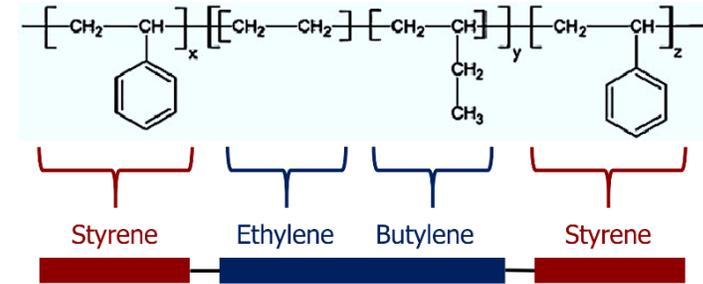
Depending on styrene content and molecular weights, phase separation induces various morphologies:

**Spherical morphology**

→ Isotropic properties

**Cylindrical morphology**

→ Anisotropic properties



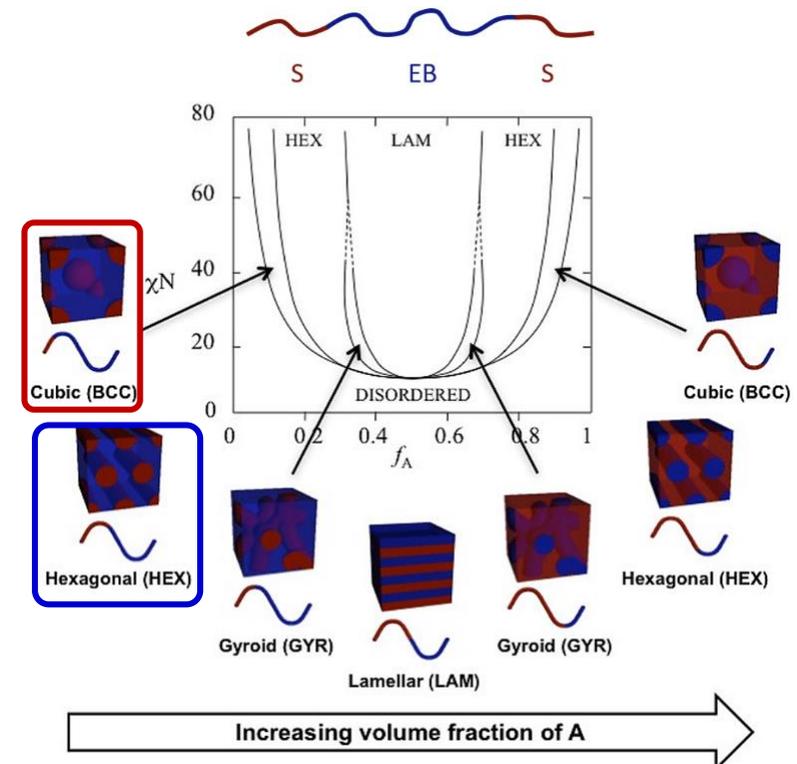
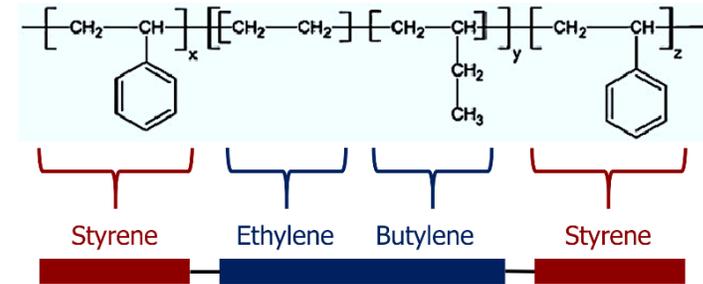
# STYRENIC THERMOPLASTIC ELASTOMERS

Depending on styrene content and molecular weights, phase separation induces various morphologies:

PoliValve: **Stent – Hard SEBS**, **Leaflets – SEBS 20**

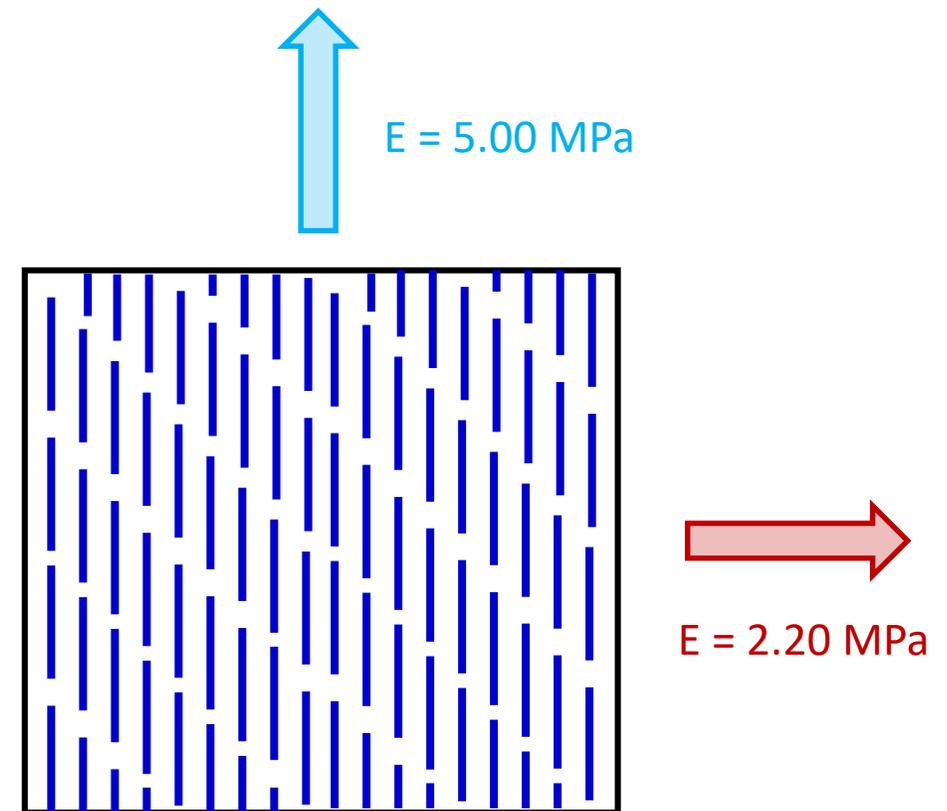
Material	Molecular weight (g/mol)	Morphology	Styrene fraction (% wt.)
Soft SEBS	High	Spherical	<20
Hard SEBS	High	Spherical	<20
SEPS-22	71, 697	Cylindrical	19.2
SEBS-29	74, 837	Cylindrical	28.4
SEBS-20	111, 327	Cylindrical	19.6
SIBS-19	High	Cylindrical	19.0

*Table of styrenic block copolymers studied for PHV application.*



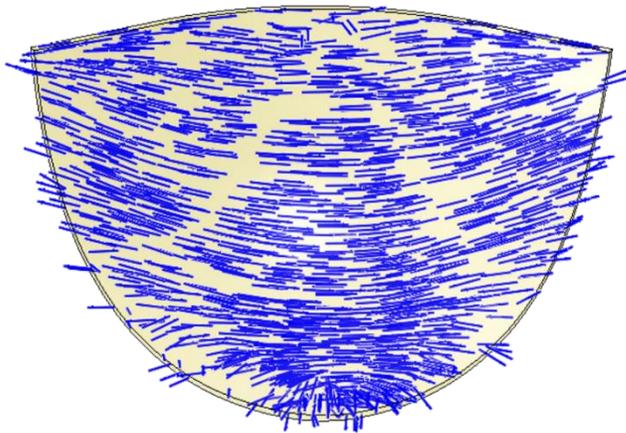
# STYRENIC THERMOPLASTIC ELASTOMERS

- Mechanical properties measured in anisotropic styrenic thermoplastic elastomers vary based on cylinder orientation
- Anisotropy is flow induced during polymer processing
- For an oriented sheet of SEBS 20 (leaflets) the Young's modulus measured for parallel and perpendicular orientation follows a 2.3 : 1.0 ratio

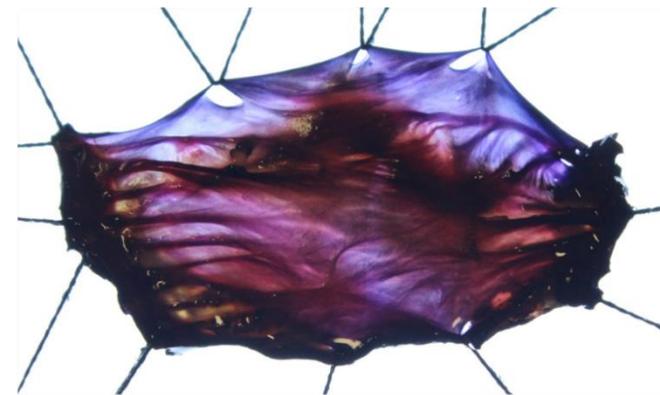


# MODELLING ANISOTROPY IN STYRENIC ELASTOMERS

- Computational modelling used to **tailor anisotropy** in the leaflet
- Optimisation shows **circumferential alignment** of cylinders along the maximum stress direction
- Orientation achieved by having **injection point at centre** of leaflet
- Fatigue lifetime model **under predicts** durability in the PHV → needs further development



Optimised cylinder orientation



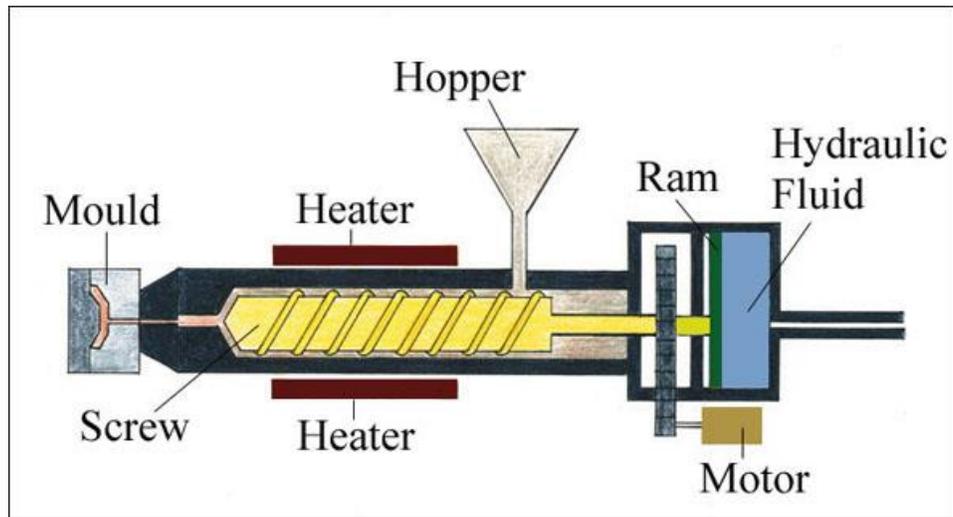
Natural tissue leaflet

- M. Serrani et al., "A Computational Tool for the Microstructure Optimization of a Polymeric Heart Valve Prosthesis," *J. Biomech. Eng.*, vol. 138, no. 6, pp. 16–20, 2016.
- J. Brubert, "A novel polymeric prosthetic heart valve: design, manufacture, and testing," p. 296, 2015.

# MANUFACTURING PROTOTYPES

## Injection moulding

- Fit moulds into machine and load polymer
- Establish screw and mould temperatures
- Optimise holding pressure and cooling procedure
- Inject polymer into mould, cool and remove part



# MANUFACTURING PROTOTYPES

## CNC Machining

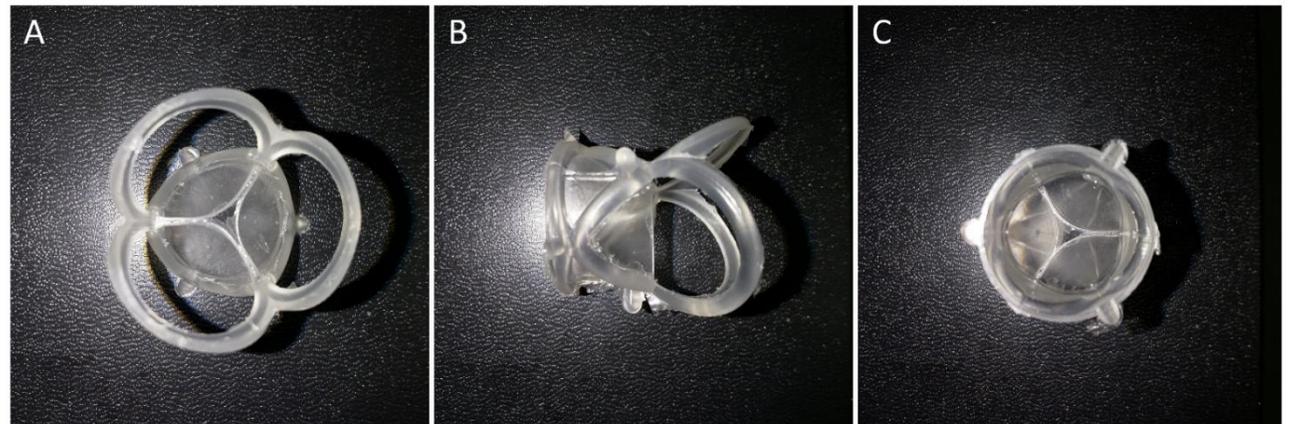
- Program tool paths
- Set up tools and stock block
- Perform machining steps



*CNC machined inserts (left), female mould (centre), male mould (right).*

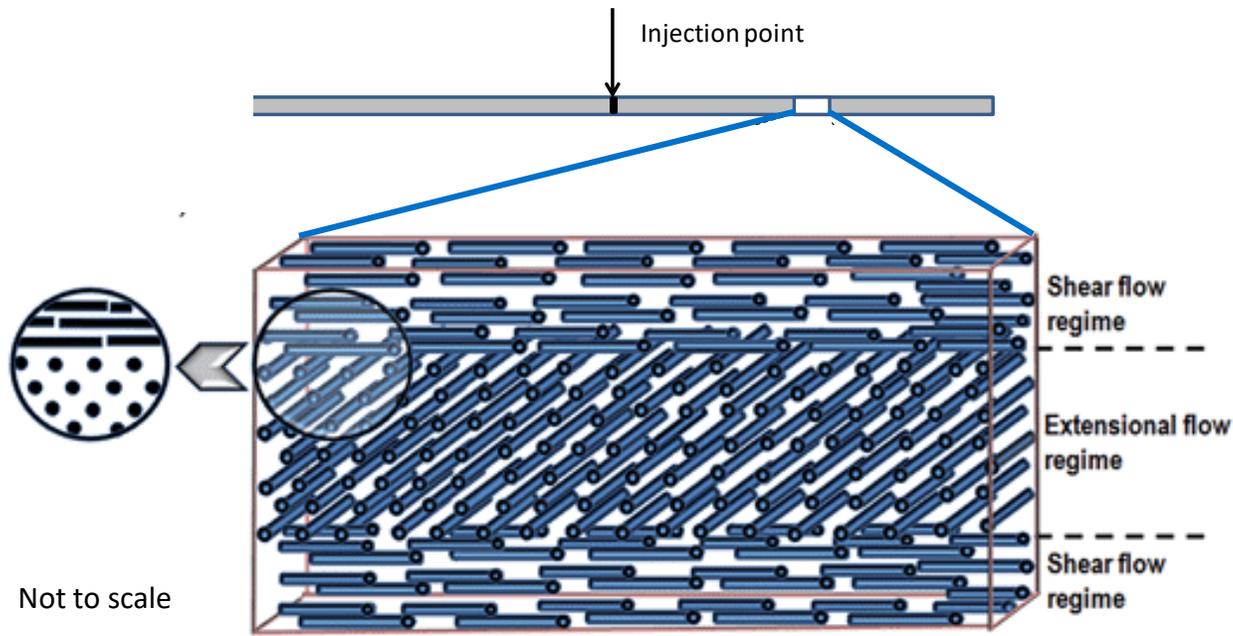
## Mold making considerations

- High quality finish
- Tolerances and undercuts
- Injection point position



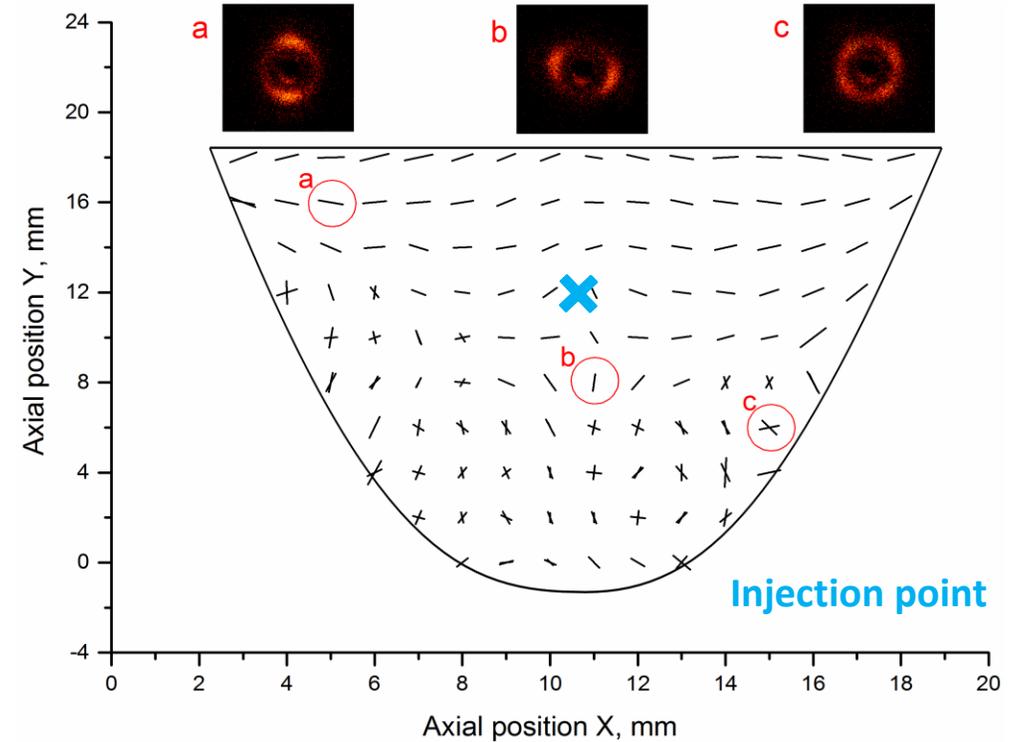
*Top view (A), side view (B) and bottom view (C) of injection moulded transcatheter PHV*

# ANISOTROPY IN PHV LEAFLET



**Alignment of cylinders in an injection moulded sample**

- J. Stasiak et al, *A bio-inspired microstructure induced by slow injection moulding of cylindrical block copolymers*, 2014.

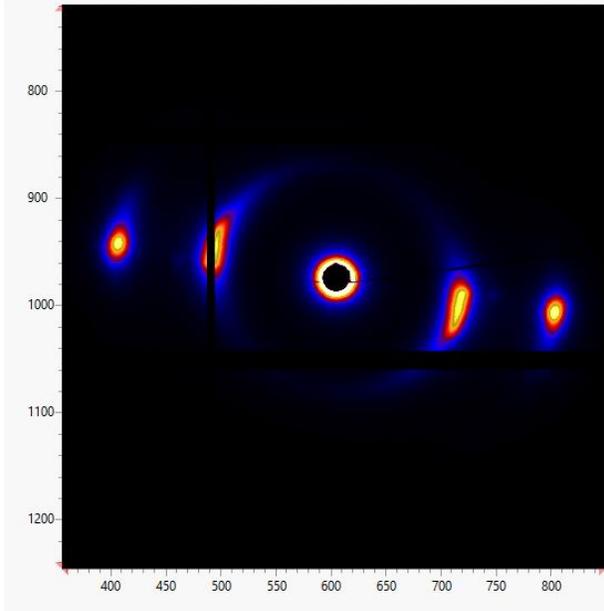


**Small angle X-ray scattering images**

- J. Stasiak et al, *Design, Development, Testing at ISO standards and in-vivo feasibility study of a novel Polymeric Heart Valve Prosthesis*, 2020.

# SMALL ANGLE X-RAY SCATTERING

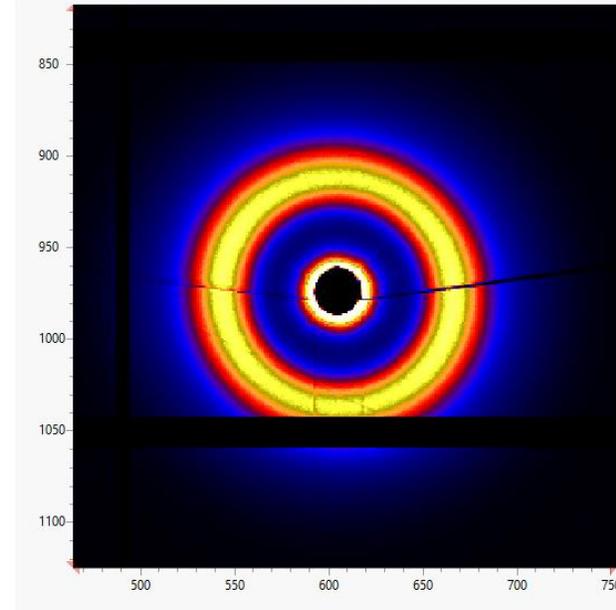
50490\_processed\_201027\_174323.nxs:/processed/result/data[0,0,0;1679;1



**Cylindrical morphology**

- SEBS 20 (leaflet)

50492\_processed\_201027\_182830.nxs:/processed/result/data[0,0,0;1679;1

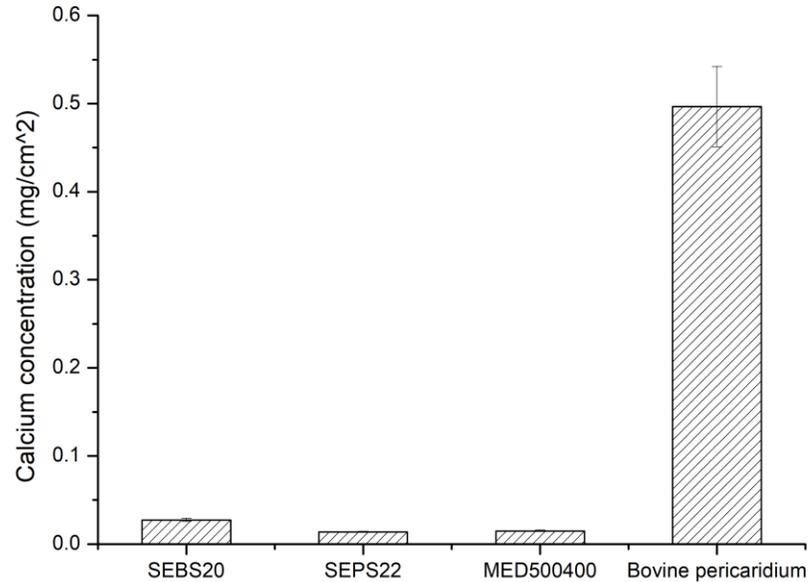


**Spherical morphology**

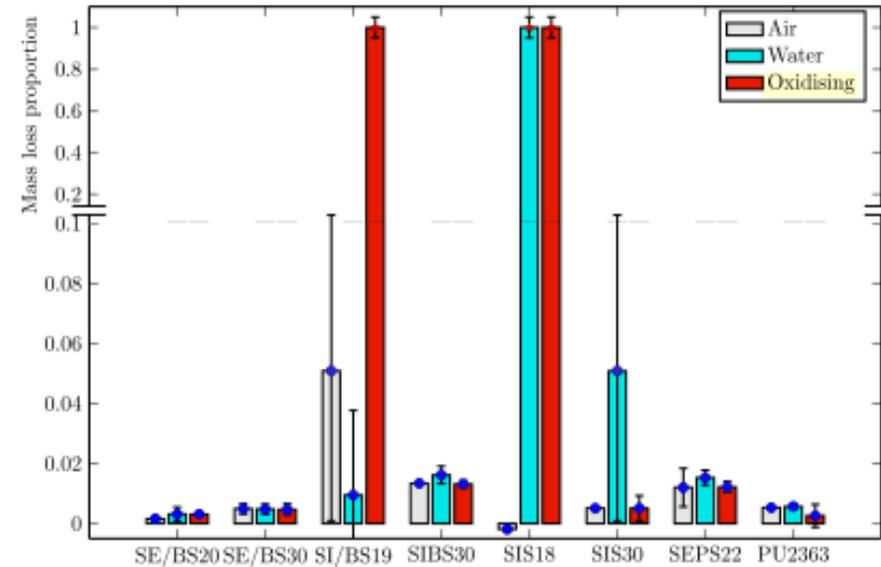
- Hard SEBS (stent)

Source: Synchrotron SAXS on beamline I22 at Diamond Light Source, Harwell, UK.

# CALCIFICATION AND OXIDATION



Significantly lower susceptibility to calcification than bovine pericardium



- Very low mass loss seen for SE/BS20 and SEPS22

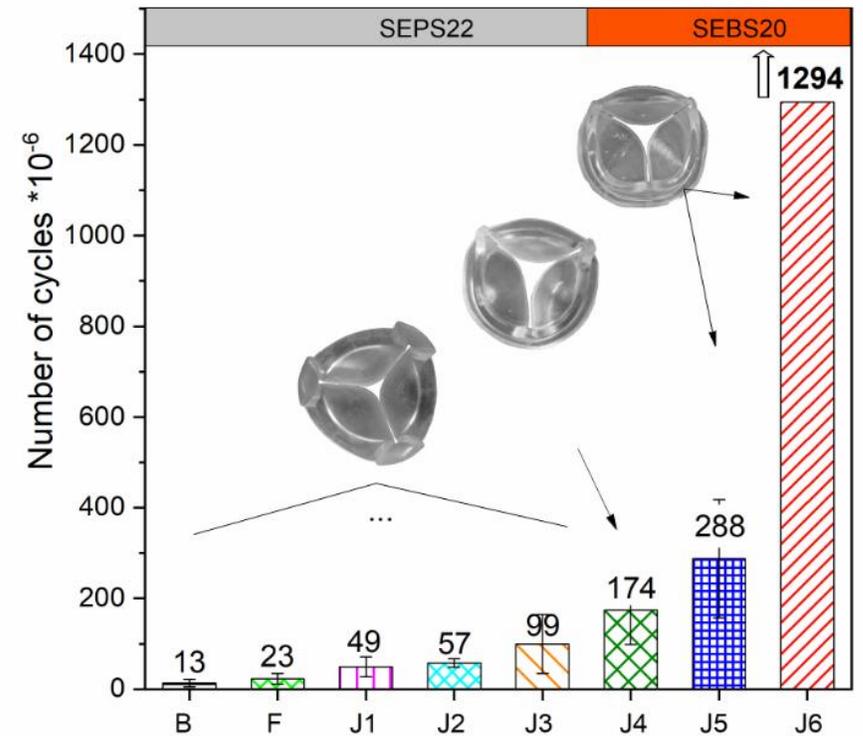
- More detailed studies on calcification and oxidation are in progress

Source: - Experiment and data collected by E. Okafor and J. Allford

- J. Brubert, "A novel polymeric prosthetic heart valve: design, manufacture, and testing.", 2015.

# POLIVALVE PERFORMANCE SUMMARY

- PHV **injection moulded** from two styrenic block copolymers
- Leaflets have **tailored anisotropic properties** that mimic the native heart valve
- **Durability** improved by adjusting injection point position, leaflet shape and adding filets around leaflets
- Latest prototype lasts > **1 billion cycles** (~25 years) under accelerated fatigue testing
- Tested **in vitro** according to ISO 5840 standards and short term **in vivo** early feasibility study



*J. Stasiak et al, Design, Development, Testing at ISO standards and in-vivo feasibility study of a novel Polymeric Heart Valve Prosthesis," 2020.*

# CONCLUSIONS & FUTURE WORK

- Styrenic thermoplastic elastomers are effective materials for flexible leaflet PHV's that are **durable** and potentially **biocompatible**
- **Flow induced anisotropy** proves to be a useful tool to enhance durability in PHV leaflets
- Styrenic thermoplastic elastomers used in the Polivalve have demonstrated **good mechanical performance** and **resistance to calcification**

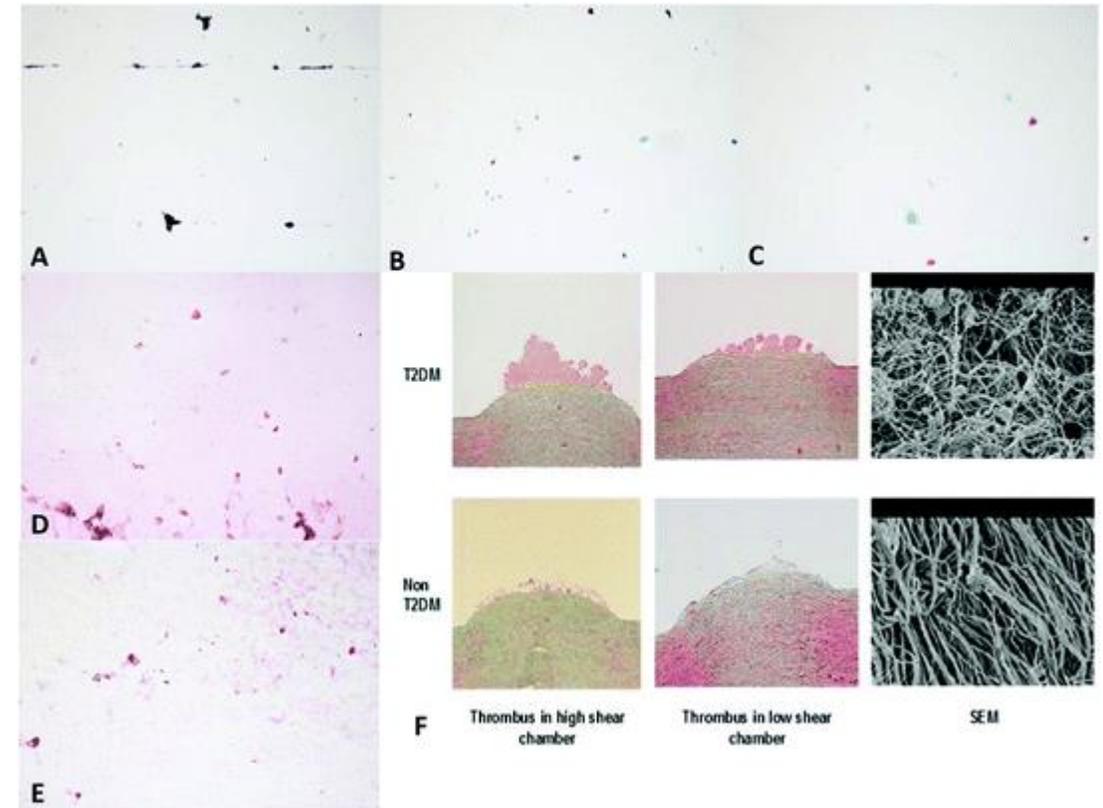
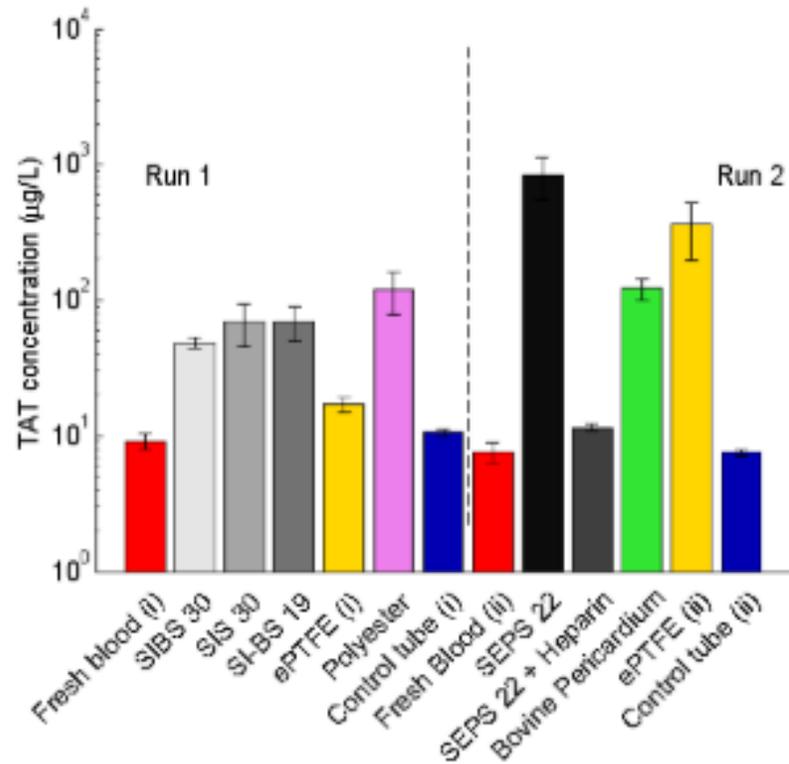
## Future work:

Continue to improve durability by studying anisotropy in styrenic block copolymers

Run tests to further study material biocompatibility (e.g. oxidation, calcification, biostability).



# HEAMOCOMPATIBILITY



Thrombin is generated in the common pathway of the coagulation cascade as measured by the concentration of thrombin-antithrombin complex